

The AsTeRICS Academy

for cross-cultural education in Assistive Technology









Module 4c: Bioelectric Signals

Processing and Classification (Basics)











Foundations of DSP Basic Operations: convolution Digital Filters: FIR and IIR Some Classification methods Biosignal Libraries and Applications

Topics

Practical Demonstrations: Matlab and FiView Review of Project exercises Firmware - programming



Recommended online book for todays topics:

The Scientist and Engineer's Guide to Digital Signal Processingby Steven W. Smith, Ph.D.http://www.dspguide.com/





In microprocessor based biomedical applications we have Signals that:

- are discrete (digitized with a sampling rate)
- are to a certian degree spoiled by noise or artifacts
- have some properties we are especially interested in
- have stochastic and sometimes nearly-deterministic behaviour



Basic Signal Statistics







Basic Signal Statistics



Histogram, Probability mass function, Probability density function:







Signals and LTI-Systems:

- Generation of an output signal in response to an input signal
- discrete and continuous systems



Linear, Timeinvariant Systems:

- additivity $x[n] \xrightarrow{System} y[n] \Rightarrow kx[n] \xrightarrow{System} ky[n]$
- homogeneity $x_1[n] \xrightarrow{\text{System}} y_1[n], x_2[n] \xrightarrow{\text{System}} y_2[n] \Rightarrow x_1[n] + x_2[n] \xrightarrow{\text{System}} y_1[n] + y_2[n]$
 - shift invariance



Foundations of DSP









• <u>Decomposition</u>: the inverse operation





Foundations of DSP - Superposition



• Any signal can be decomposed into a group of additive components xi

• Passing these components through a linear system produces signals, *yi*



• The *synthesis* of these output signals produces the same signal as when *x* [*n*] is passed through the system

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- combined two signals into a third one
- applies a linear system to a signal via it's impulse response, wich fully describes the system behaviour





$$y[i] = x[i] * h[i] \Leftrightarrow y[i] = \sum_{j=0}^{M-1} h[j]x[i-j]$$
 M .. length of impulse response



Foundations of DSP – Convolution

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Application of a LTI:

- 1) multiplication of the input samples with the <u>flipped</u> impulse response
- 1) addition of the values gives result for the corresponding output sample







- many samples of the input signals contribute to one output sample
- the samples of the impulse response act as weighing coefficients
- feeding a delta function into a linear system gives the impulse response:







• simple implemenation of convolution:





Relationships between impulse-, step- and frequency response:



Note: Convolution in time domain = multiplication in frequency domain !





The shape of the impulse response determines phase- and frequency response of an LTI system. The impulse response is also called "filter kernel".

- Finite Impulse Response Filters can be implemented by a single convolution of an input signal with the filter kernel
- Several positive vaules in the impulse response give an averaging (low-pass) filter
- Substracting a low-pass filter kernel from the delta function gives a high pass filter kernel
- A symmetrical impulse response gives a linear phase response





Example High and Lowpass Filter-Kernels:







• Digital Filters can be described by the generalized discrete differential equation:

$$\sum_{m=0}^{M} a_{m} \cdot y[n-m] = \sum_{k=0}^{N} b_{k} \cdot x[n-k]$$

a, b : filter coefficients x[n] : input signal y[n] : output signal M,N : filter order

the <u>right side</u> depends only on the inputs x[n] : feed-forward the <u>left side</u> depends on the previous outputs y[n] : feed-back

FIR Filters have only feed-forward components, they can be calculated non-recursively, by convolution

IIR Filters have feed-back components also, they are calculated recursively (infinite impulse response)



can be described by the transfer function:

$$\begin{split} \sum_{m=0}^{M} a_m \cdot y[n-m] &= \sum_{k=0}^{N} b_k \cdot x[n-k] \quad \left| \xleftarrow{Z} \right\rangle \quad Y(z) \cdot \sum_{m=0}^{M} a_m \cdot z^{-m} = X(z) \cdot \sum_{k=0}^{N} b_k \cdot z^{-k} \\ H(z) &= \frac{Y(z)}{X(z)} = \frac{\sum_{k=0}^{N} b_k \cdot z^{-k}}{\sum_{m=0}^{M} a_m \cdot z^{-m}} \end{split}$$

- z^x in Z-domain represents a delay element of x discrete delays,
- the numerator describes the feedfoward part of the filter, 0 = "zeros"
- the denumerator describes the feedback part of the filter, 0 = "poles"





$$y[n] = \sum_{k=0}^{N} b_k \cdot x[n-k]$$

- finite impulse response, no recursion
- described by multiplication coefficients
- less sufficient (need higher order)





Digital Filters – IIR filters



$$y[n] = \sum_{k=0}^{N} b_k \cdot x[n-k] + \sum_{m=1}^{M} -a_m \cdot y[n-m]$$

- infinite impulse response, truncated at a certain precision
- use previously calculated values from the output (recursion)
- described by recursion coefficients
- more efficient, but can be unstable





Filter characteristics



POOR 1.5 1.5 a. Slow step response 1.0 1.0 Amplitude Amplitude 0.0 0.0 -0.5 --0.5ó 16 32 48 б4 0 Sample number 1.5 1.5 c. Overshoot 1.0 1.0 Amplitude Amplitude 0.5 0.0 0.0 -0.5 -0.5-32 ó 16 48 64 Sample number 1.5 1.5 e. Nonlinear phase 1.0 1.0 0.5







Performance in Time Domain





Filter characteristics



0.5

POOR 1.5 a. Slow roll-off 1.0 Amplitude 0.0 -0.5 ò 0.1 0.2 0.3 0.4 0.5 Frequency 1.5 c. Ripple in passband 1.0 Amplitude 0.0 -0.5 -0.1 0.2 0.3 0.4 0.5 Ó Frequency 40 e. Poor stopband attenuation 20-







Performance in Frequency Domain





typical IIR filters





Chebyshev, Butterworth and Bessel characteristics



Implementation Considerations



- floating point multiplication in uCs is usually very slow
- many uCs provide hardware multipliers and fast MAC operations
- fractional number arithmetics speed up filter calculation scale the input data and coefficients to get the needed precision, use integer multiplication, shift back the result:



Issues:

- scaling factor / register size (overflow ?)
- resulting resolution

Atmel Application note AVR223 – Digital Filters with AVR

http://www.atmel.com/dyn/resources/prod_documents/doc2527.pdf







60 Hz notch example

Frequencies that define complex zeros:

f0=60Hz - power supply frequency fs=500Hz - sampling rate

we get w0 = 0.754

Positions of complex zeros:

$$z_1 := \cos (\omega_0) + j \cdot \sin (\omega_0)$$
$$z_2 := \cos (\omega_0) - j \cdot \sin (\omega_0)$$





Matlab-source: http://www.scienceprog.com/category/biomedical-dsp



Digital FIR Filters



60 Hz notch filter example

System Function:

$$H(z) = \frac{Y(z)}{X(z)} = \frac{(z - z_1)(z - z_2)}{z^2}$$

$$\frac{(z - z_1) \cdot (z - z_2)}{z^2} = \frac{z^2 - z \cdot z_2 - z_1 \cdot z + z_1 \cdot z_2}{z^2} = 1 - z^{-1} \cdot (z_2 + z_1) + z^{-2} \cdot z_1 \cdot z_2$$

$$1 + z^{-1} \cdot (-2 \cdot \cos(\omega_0)) + z^{-2}$$
Filter Coefficients:

$$b_3 := 1 \quad b_2 := -2 \cdot \cos(\omega_0) \quad b_1 := 1$$

$$X(n)$$



 $G := \frac{1}{(2 - 2 \cdot \cos(\omega_0))}$ scaling: G = 1.845



Digital FIR Filters



60 Hz notch filter example



Resulting Filter characteristics



Filter Design with Matlab / Simulink



```
h= fdesign.bandpass('N,Fc1,Fc2', N, Fc1, Fc2, Fs);
Hd = design(h, 'butter');
y=filter(Hd,x);
```

```
b = fir1(N, Fc/(Fs/2), 'high', win, flag);
Hd = dfilt.dffir(b);
y=filter(Hd,x);
```

```
[b,a]= butter (N,0.1,'high');
y=filter(b,a,x);
```

- Filter Design and Analysis Tool (fdatool)
- Signal Processing Toolbox
- Simulink Signal Processing Blocksets:



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60Hz notch applied to ECG signal





```
fid = fopen('ekg.txt','r');
InputText=textscan(fid,'%f',1500,
'delimiter','\n');
x=cell2mat(InputText);
fclose(fid);
subplot(2,1,1);
plot(x);
```

```
[b,a]= butter (2,0.1,'high');
% 0.1 = 12,8 Hz at 256 Hz
y=filter(b,a,x);
```

```
subplot(2,1,2);
plot(y);
```

Example file: read_file_filter.m



highpass for ECG, signal parsed from a text file







Fdatool: Filter Design and Analsys, export to Simulink / Workspace









Filter Application and Test in a Simulink Model

Example file: filtertest.mdl





- written by Jim Peters, part of the OpenEEG Source pool
- cross platform compatible (using SDL-Library)
- graphical comparison of different filters, testing with feed-signals
- example invocation for a 4-filter comparison: fiview 256 -f 10 -i LpBe4, LpBe6, LpBu4, LpBu8
- generates source code (C functions)
- templates for standard filter types, creation by coefficients

Download Link http://uazu.net/fiview/





Other Signal Processing Techniques





 same operation as convolution, but non-flipped multiplication

Correlation

- finds similar signals in a signal (cross correlation)
- finds perodic parts of a signal (auto-correlation)





Discrete Fourier Transform







Discrete Fourier Transform

Amplitude



Re $X[k] = \sum_{i=0}^{N-1} x[i] \cos(2\pi ki/N)$ Im $X[k] = \sum_{i=0}^{N-1} x[i] \sin(2\pi ki/N)$

• Inverse Transform:

$$x[i] = \sum_{k=0}^{N/2} \operatorname{Re} X[k] \cos(2\pi k i / N) + \sum_{k=0}^{N/2} \operatorname{Im} X[k] \sin(2\pi k i / N)$$

• FFT-Algorithms:

FFTW, FFTPACK, Green, Ooura, Sorensen







• Calculation of Magnitude and Phase response:

 $MagX[k] = \sqrt{(\operatorname{Re} X[k]^2 + \operatorname{Im} X[k]^2)}$

$$PhaseX[k] = \arctan\left(\frac{\operatorname{Im} X[k]}{\operatorname{Re} X[k]}\right)$$







Discrete Fourier Transform - Problems



Stationary signal: correct representation of 4 frequency-components





Problems with non-stationary signals

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• Solution: Short Term Fourier-Transform: windowing is used to analyse small portions of (aperiodic) signals







• Problem with Short Term Fourier-Transform: window-size is fixed and determines tradeoff in resolution betewwn time and frequency:





Wavelet Transformation



- good frequency resolution at low frequencies and
- good time resolution at high frequencies
- no work-around for the principle of entropy









- scale (s) and translation (t) of the base wavelet
- convolution with the signal
- special wavelets for special purposes











A quick glance at

Classification - Methods





- Input data: time or frequency domain characteristics
- purpose: clustering, event detection, data reduction
- get "semantic information" out of our data
- achive a high detection rate -> few false-positive or false-negative classifications
- feature extraction is used to handle huge amounts of data
 reduce the feature space





Simple classification could be based on:

- Thresholds (levels / intervals, adaptive thresholds)
- absolute values + averaging over intervals
- integration / difference
- local minima / maxima, zeros in time domain
- Energy, energy distribution over frequency bands



Classification - Methods



Neural Networks:

- mimic biological signal processing
- Input-, hidden and output-layers units with activation functions
- learning algorithms e.g. error back propagation unsupervised learning / clustering
- internal representation unrevealed
- pattern recognition, predicition





Principal Component Analysis and Independent Component Analysis:

- reduction of complexity of the feature-space
- singular-value decomposition delivers component functions (base-functions) that can restore the relevant information with less features
- ICA: non-orthogonal base functions allowed, used for blind-source separation EEG: artefact removal, signal source models



http://www.eurekalert.org

Scott Makeig: http://www.sccn.ucsd.edu/~scott/





Suport Vector Machines (SVMs):

- binary classificatin of an input vector
- training with classified data seperates the feature space in two areas, with maximal distance of positive / negative classifications
- SVMs find a global minimum (in contrast to e.g. neural networks)







EEGLab:

- Matlab-based, open source application
- 300 functions for data analysis and feature extraction e.g: epoch based ERP averaging ICA-methods for source localisation handling of MRI-data
- imports command file formats like EDF, BDF, ...

http://www.sccn.ucsd.edu/eeglab/









Tempo:

- Topographic EEG Mapping Program (open source)
- 3d display of MRI head models,
- generates animated sequences
- imports EDF

http://tempo.sourceforge.net/









BioExplorer:

- Real-time biosignal aquisition, analysis and classification
- FFT, filtering, correlation, adaptive thresholding
- File operations
- visual and acoustic biofeedback
- compatible with OpenEEG-hardware



http://www.cyberevolution.com/





BWView:

- Wavelet-based signal analysis tool using fft-accelerated convolution
- open source
- compatible to OpenEEG-hardware

http://uazu.net/bwview/



Respiratory sinus arrythmia (RSA) seen with BWview http://jhansmann.de/eeg/experiments/index.html





FiView and FidLib – IIR filter design tool by Jim Peters

http://uazu.net/fidlib/



Frequency response and Impulse response, calculated and viewed with FiView





FiView and FidLib – IIR filter design tool by Jim Peters

```
// Example code (readable version)
double
process(register double val) {
   static double buf[4];
   register double tmp, fir, iir;
   tmp= buf[0]; memmove(buf, buf+1, 3*sizeof(double));
   val *= 0.0006918804381787758;
   iir= val+1.496016726996244*buf[0]-0.6177887989473995*tmp;
   fir= iir+buf[0]+buf[0]+tmp;
   tmp= buf[1]; buf[1]= iir; val= fir;
   iir= val+1.415382337323265*buf[2]-0.5062905959533784*tmp;
   fir= iir+buf[2]+buf[2]+tmp;
   buf[3]= iir; val= fir;
   return val;
```

Example Filter code for a butterworth IIR filter, generated with FiView





```
#include "fidlib/fidlib.h" // May need adjusting
FidFilter *
setup() {
   FidFilter *filt0= fid design("LpBe4", 256, 10, 0, 0);
   return filt0;
}
   FidFilter *filt= setup(); // Run a couple of instances using fidlib
   FidFunc *funcp;
   FidRun *run= fid run new(filt, &funcp);
   void *fbuf1= fid run newbuf(run);
   void *fbuf2= fid run newbuf(run);
   while (...) {
      out 1= funcp(fbuf1, in 1);
      out 2= funcp(fbuf2, in 2);
      if (restart required) fid_run_zapbuf(fbuf1);
      . . .
   fid run freebuf(fbuf2);
                                         FidLib C-library provides efficient
   fid run freebuf(fbuf1);
                                         generic filter creation at runtime
   fid run free(run);
```





EngineerJS: Online JavaScript IIR filter design Tool



http://engineerjs.com/?sidebar=docs/iir.htm